The accuracy of transcutaneous PCO₂ in severe brain injury patients: a comparison with end-tidal PCO₂

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Financial support: None

Conflict of interest: All authors state that there is no conflict of interest.

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RESPIRATORY CARE Paper in Press. Published on December 03, 2013 as DOI: 10.4187/respcare.02726

Abstract

Background: In patients suffering from brain injury, end-tidal PCO₂ (P_{ET}CO₂) monitoring is controversial but

transcutaneous PCO₂ (PtcCO₂), which is noninvasive and utilizes real-time display, may be an alternative

method. We hypothesized that PtcCO₂ would be more accurate than P_{ET}CO₂ for monitoring PaCO₂ in severe

brain injury patients.

Methods: A prospective observational study included consecutive mechanically ventilated adult subjects who

had acute brain injury and an arterial catheter in place. When an arterial blood gas analysis was required, the

PETCO2 and PtcCO2 values were simultaneously recorded. The agreement between the PETCO2, PtcCO2 and

arterial PCO2 (PaCO₂) measurements (reference) was determined using the Bland-Altman method. The number

of outliers defined by the formula ([P_{ET}CO₂ or PtcCO₂] - PaCO₂) > ± 4 mmHg indicated the proportion of

measurements that were considered clinically unacceptable.

Results: A total of 25 subjects were included in the study, and 85 simultaneous measurements of PaCO₂,

PtcCO₂ and P_{ET}CO₂ were obtained. The bias and precision between PaCO₂ and PtcCO₂ were -0.75 and 6.23

mmHg, respectively. The limits of agreement ranged from -12.97 to 11.47 mmHg. The bias and precision

between PaCO₂ and P_{ET}CO₂ were 0.68 and 5.82 mmHg, respectively. The limits of agreement ranged from

-10.72 to 12.08 mmHg. There were 34 (40%) outliers for the PtcCO₂ sensor and 34 (40%) outliers for the

 $P_{ET}CO_2$ sensor (P = 1).

Conclusions: The accuracy of PtcCO₂ was not superior to that of P_{ET}CO₂ for assessing PCO₂ levels and should

not be used to monitor these levels in severe brain injury subjects.

Key words: Respiratory monitoring, end-tidal PCO₂, transcutaneous PCO₂, brain injury, accuracy.

Acknowledgments: none

Introduction

Patients who suffer from a brain injury require maintaining blood carbon dioxide pressure (PCO₂) within the physiological range to avoid cerebral spinal fluid pH change and prevent cerebral vasodilatation and vasoconstriction [1]. The "gold standard" technique for monitoring PCO₂ is the determination of arterial PCO₂ (PaCO₂) using arterial blood gas. However, the arterial blood gas test is time-consuming, requires a significant amount of blood, must be repeated, particularly in brain injury patients, and does not display real-time data.

Therefore, techniques that can avoid these pitfalls are needed. End-tidal PCO_2 ($P_{ET}CO_2$) is a non-invasive tool that allows for the continuous monitoring of PCO_2 . However, in subjects with severe brain injuries, the use of $P_{ET}CO_2$ as a surrogate of $PaCO_2$ has been disappointing [2-5]. Therefore, $P_{ET}CO_2$ is only recommended for use in out-of-hospital settings when arterial blood gas is not available [6-8].

New devices that measure transcutaneous PCO₂ (PtcCO₂) have recently become available. The general principle of PtcCO₂ measurement is that CO₂ diffuses from capillary through tissue and across the semi-permeable membrane of the device sensor, which is a modified Severinghaus electrode [9]. The agreement between the measured PtcCO₂ and PaCO₂ is dependent on the high tissue solubility of CO₂, which is further promoted by warming of the skin under the electrode. However, studies of this technology in intensive care units have produced conflicting results, with accuracy varying between studies according to the type of subjects who were evaluated [10-14]. In studies that have compared both PtcCO₂ and P_{ET}CO₂ to blood gas-measured PaCO₂, the former technology does appear to be more accurate [15,16].

In this study, we hypothesized that $PtCO_2$ would be more accurate than $P_{ET}CO_2$ in predicting $PaCO_2$ in brain injured patients. Therefore, we compared simultaneous $PtcCO_2$ and $P_{ET}CO_2$ values to the reference $PaCO_2$ value in brain injury subjects.

Methods

This prospective observational study was performed at the surgical ICU of a university hospital from June 2011 to January 2012. The study was approved by the local ethics committee, which waived the requirement for informed consent from subjects or their relatives (law relative to the French public health policy no. 2004-806 – Ethics Committee, CHU de Rennes, avis n°12.03).

Consecutive mechanically ventilated subjects who were >15 years of age, had a brain injury (Glasgow Coma Scale \leq 8), had an arterial catheter in place and required arterial blood gas were included.

All brain injury patients were managed according to standardized protocols in order to maintain a mean arterial pressure (MAP) \geq 85mm Hg, an ICP \leq 20mm Hg, and a cerebral perfusion pressure (CPP) \geq 65mm Hg [1]. Other types of therapy to avoid secondary insults were applied as recommended [1]. In patients suffered from subarachnoid hemorrhage, MAP was maintained \geq 90 mmHg. All patients were in a semi-recumbent position (>30°) and received sedatives agents but none were paralyzed.

The following data were recorded during the first 24 hours of admission to the ICU: age, sex, body weight, the nature of the brain injury, the Glasgow Coma Scale upon admission, the Simplified Acute Physiology Score II and the Sequential Organ Failure Assessment score. Norepinephrine was administered when necessary, and the dose was recorded. For each comparison, the following variables were reported: the body core temperature, the tidal volumes, the respiratory rates, the use and level of positive end expiratory pressure (PEEP), the presence of mottling on the legs, the capillary refilling time, the arterial pH, and the hemoglobin level provided by the arterial blood gas analysis.

When the inclusion criteria were met and arterial blood gas measurement was ordered, the $PtcCO_2$ and $P_{ET}CO_2$ were simultaneously recorded.

Carbon dioxide measurement

Arterial blood gas was sampled using an arterial catheter (Seldicath 3F, Plastimed-Prodimed, Le Plessis Bouchard, France) in a heparinized syringe and assessed using an analyzer (700/800 series, Radiometer Medical ApS, Brønshøj, Denmark). PtcCO2 was measured using the SenTec monitor via a V-SignTM Sensor (Sentec AG,

Therwil, Switzerland) according to the manufacturer's instructions. All of the measurements were taken at the right or left earlobe. The V-sign Sensor was inserted into the docking station of the monitor, and the calibration was automatically performed. Then, the V-sign Sensor was clipped into the multi-site attachment at the earlobe ring. The earlobe was chosen because it appeared more accurate than the forehead or cheek [13]. The quality of the signal was estimated by the pulsatility index provides by the Sentec monitor (normal range: 1 to 2). As a warm-up period (≈ 30 min) is necessary for the electrode to reach its optimal working conditions, all of the measurements were performed after this period.

P_{ET}CO₂ was measured via a non-aspirated infrared capnograph (M1460A, Hewlett Packard, Andover MA, USA), which was inserted at the tip of the tracheal tube and connected to a multi-parameter monitor (SC 9000 XL; Siemens Elema AB, Solna, Sweden). The quality of the P_{ET}CO₂ measurement was the visualization on the monitor of a typical waveform with a rapid and abrupt inspiratory/expiratory segments separated by a near horizontal alveolar plateau. All of the measurements were taken at least 30 minutes after any modifications in the mechanical ventilation parameters and/or changes in the norepinephrine rate.

Statistical analysis

To demonstrate the superiority of PtcCO₂ compared with $P_{ET}CO_2$, at least 82 measurements were required (NQuery Advisor 6.0, Statistical Solutions Ltd., Cork, Ireland) assuming an α -risk of 0.05, a β -risk of 0.2, and a proportion of outliers of 40% and 20% in the $P_{ET}CO_2$ and PtcCO₂ groups, respectively [4]. The PaCO₂ value obtained by arterial blood gas was the reference value. The statistical analysis was performed using SAS version 9.3 software (SAS Institute, Cary, NC, USA). Data were expressed as the mean±SD and median (interquartile range) for the non-normally distributed variables and as the n (percentage). The agreement between the 2 measurement methods was assessed using a Bland-Altman analysis [17]. The study design included several measurements per patient; therefore, a correction was used in the limits of agreement calculation [18]. The outliers were defined as the differences $PaCO_2 - PtcCO_2$ or $PaCO_2 - PtcCO_2$ that strictly exceeded ±4 mmHg. In addition, variables which may explain the outliers for $PaCO_2 - PtcCO_2$ and $PaCO_2 - PtcCO_2$ were studied and compared using a Student's t-test or a Kruskal-Wallis test when necessary. The body temperature, the hemodynamic parameters (capillary refilling time, presence of mottling on the legs, and norepinephrine dose),

the arterial pH, and the hemoglobin level were compared between $PaCO_2$ - $PtcCO_2$ non outliers and outliers. The body temperature, the ventilation parameters (respiratory rates, tidal volumes, PEEP), the hemodynamic parameters (capillary refilling time, mottling on the legs, and norepinephrine dose), the arterial pH, and the hemoglobin level were compared between $PaCO_2$ - $P_{ET}CO_2$ non outliers and outliers.

Results

Twenty five subjects were included, and 85 simultaneous measurements of $PaCO_2$, $PtcCO_2$ and $P_{ET}CO_2$ were obtained. The baseline patient characteristics are provided in Table 1. The median number of measurements per patient was 4 (range: 1-5), and all the measurements were performed at the acute phase in the first 48 h after admission in ICU. Body core temperature, ventilation parameters, arterial pH and haemoglobin level measured at each comparisons are provided in Table 2.During the measurements, all of the subjects received a norepinephrine infusion at a mean dose of $0.4\pm0.5~\mu g/kg \cdot min^{-1}$.

A comparison of the PCO_2 measurements using arterial blood gas and the $P_{ET}CO_2$ and $PtcCO_2$ measurements are presented in Table 3. The number of outliers did not vary between the $PtcCO_2$ and $P_{ET}CO_2$ measurements. The regression analysis and the results of the Bland-Altman analysis are provided in Table 2 and Figure 1. Variables which may explain the outliers for $PaCO_2$ - $PtcCO_2$ and $PaCO_2$ - $PetcCO_2$ are provided in Table 4 and 5, respectively. There were no difference between non outliers and outliers.

Discussion

In this population of severe brain injury subjects, $PtcCO_2$ was not superior to $P_{ET}CO_2$ and could not be used as a surrogate of $PaCO_2$. The percentage of outliers was high and did not vary between the 2 measurement methods. The use of $P_{ET}CO_2$ as a surrogate of $PaCO_2$ in the ICU is controversial. Kerr et al. compared $P_{ET}CO_2$ with $PaCO_2$ in traumatic brain injury (TBI) subjects and found a bias of 1 mmHg and limits of agreement that ranged from -5.2 to +17.2 mmHg, but no clinical limits of agreement were defined [3]. In 21 TBI subjects, the bias was 5.5 mmHg, and the limits of agreement ranged from -4.5 to +15.5 mmHg [4]. The values that were considered clinically relevant were ± 4 mmHg; therefore, $P_{ET}CO_2$ could not be used to substitute for $PaCO_2$. Moreover, the $PaCO_2 - P_{ET}CO_2$ differences in 40% of the cases were outside of the previously defined limit. Recently, Lee et al. found values that were outside of the limit of ± 5 mmHg in 23% of TBI subjects [5].

The use of the SenTec monitor in ICUs has produced contrasting data. Rodriguez et al. evaluated this monitor in 50 ICU subjects who were hospitalized for various reasons [10]. The bias was -0.2 mmHg, and the limits of agreement ranged from -9.4 mmHg to +9.0 mmHg. The authors concluded that the PtcCO₂ measurement was an acceptable tool for monitoring PCO₂, but they did not consider predefined limits. Bolliger et al. compared the SenTec and TOSCA 500 monitors in 50 ICU subjects [11]. For the SenTec and TOSCA 500 monitors, the bias was -2.60 and -2.75 mmHg, and the limits of agreement ranged from -14.1 to +8.8 mmHg and -11.5 to +7.2 mmHg, respectively. According to the predefined limit of ±7.5 mmHg, the authors concluded that the 2 devices were inaccurate. Baulig et al. evaluated the SenTec monitor in cardiac surgery subjects [12]. The bias was 0.37 mmHg, and the limits of agreement ranged from -9.0 to +9.75 mmHg. Using a recently available sensor, they found a bias of 1.1 mmHg and limits of agreement that ranged from -3.4 to +5.5 mmHg, with a predefined limit of ±5 mmHg [13]. In a study that evaluated the TOSCA 500 monitor including 55 subjects, of whom 10 were multiple traumatic and neurosurgical subjects, the bias was 1.2 mmHg, and the limits of agreement ranged from -10.5 to +13.0 mmHg [14]. Nevertheless, in the subgroup of brain injury subjects, the authors concluded that PtcCO₂ should be used with caution [14].

Few studies have evaluated simultaneous measurements of P_{ET}CO₂ and PtcCO₂ using the PaCO₂ measurement as a reference [15, 16]. During general anesthesia, the values obtained with the transcutaneous PCO₂ monitor

RESPIRATORY CARE Paper in Press. Published on December 03, 2013 as DOI: 10.4187/respcare.02726

had a lower bias and narrower limits of agreement than those obtained with the end-tidal PCO₂ monitor (0.19 vs.

-4.40 mmHg and -4.6 to 4.9 mmHg vs. -10.7 to +2.9 mmHg, respectively) [15]. In mechanically ventilated

subjects who required inter-hospital transport, Hinkelbein et al. found that the bias for the end-tidal

measurement was higher than that obtained with PtcCO₂ (-5.3 vs. -0.6 mmHg) [16].

According to the a priori better performance of PtcCO2, we expected that PtcCO2 would be more accurate than

P_{ET}CO₂. We considered that acceptable differences between PtcCO₂ or P_{ET}CO₂ and PaCO₂ would not exceed ±4

mmHg as previously considered to be clinically relevant in studies of brain injury subjects [4, 5, 19]. The

percentage of outliers using the SenTec monitor did not differ from those that were associated with the P_{FT}CO₂

measurement and the limits of agreement were significant, which suggests that the PtcCO2 measurement should

not be used in subjects suffering from brain injury.

Our study has some limitations that must be pointed out. Indeed, it may be argued that norepinephrine may have

modified the skin perfusion and PtcCO₂ values. These subjects often require at the acute phase such medication

to maintain adequate cerebral perfusion pressure and/or MAP [1]. Nevertheless, the relationship between

vasopressor use and an alteration in the bias and precision has not been demonstrated and in our study, no

relationship was found between the norepinephrine dose and the difference between PaCO₂ and PtcCO₂ [14, 20].

We measured PtcCO₂ at the earlobe and we cannot exclude regional hypoperfusion, although the earlobe site

was found to provide the better accuracy [13].

In conclusion, PtcCO₂ measured at the earlobe with the Sentec monitor was not superior to P_{ET}CO₂ in subjects

who were suffering from brain injury and should not be used to monitor PCO₂ in these subjects.

Acknowledgements: None

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Figure Legend

Figure 1. Bland-Altman agreement between arterial PCO_2 and $PtcCO_2$ (A) and between arterial PCO_2 and $PtcCO_2$ (B).

Table 1. Patient characteristics.

Patients	n = 25
Age, years	46 [31–52]
Sex, male	13 (52)
Nature of the brain injury	
Trauma	16 (64)
Subarachnoid hemorrhage	3 (12)
Other*	6 (24)
SAPS II	43 [36–52]
SOFA score	8 [7–9]
Glasgow Coma Scale upon admission	6 [4–7]

The data are presented as the median [interquartile 25–75] and number (%). SAPS II: Simplified Acute Physiology Score II. SOFA: Sequential Organ Failure Assessment. *Other: stroke (n = 2), intracranial hemorrhage (n = 2), brain abscess (n = 2), and tumor (n = 1).

Table 2. Body core temperature, ventilation parameters, hemodynamic parameters, arterial pH and hemoglobin level for each comparison (n=85).

Body core temperature, °C	37.8±0,8 [36.7 – 40.7]*
Ventilation parameters	
- Tidal volume, ml/kg	7.8±1.2
- Respiratory rate,	13±3
- PEEP, n(%)	59 (69%)
- Level of PEEP, cm H ₂ O	3±2
Mottling, n(%)	40 (47%)
Capillary refilling time, sec†	2 (1-3)
Arterial pH	7.41±0.06
Hemoglobin, g/dl	9.5±1.4

Values are expressed as mean±SD unless overwhise. *[minimum – maximum]. † Missing data, n=2. PEEP: Positive end expiratory pressure.

Table 3. Arterial, transcutaneous and end-tidal carbon dioxide pressure values, linear regression and the Bland-Altman analysis results ($PtcCO_2$ or $P_{ET}CO_2$ vs. $PaCO_2$) and number of outliers.

	Linear regression						
	PCO ₂ values	Bland-Altman analysis			ysis	Outliers	
_	(mmHg)	Coefficient correlation	р	Bias* (mmHg)	Precision (mmHg)	Limits of agreement (mmHg)	n (%)
PaCO ₂	37.0 ± 6.2 (23.0; 53.0)			-	-		
PtcCO ₂	37.7 ± 7.2 (24.1; 61.3)	0.60	< 0.001	-0.75	6.23	-12.97; 11.47	34 (40%)
$P_{ET}CO_2$	36.3 ± 6.7 (22.0; 52.0)	0.58	< 0.001	0.68	5.82	-10.72; 12.08	34 (40%)

The data are presented as the mean \pm SD (min; max) and number (%). PCO₂: carbon dioxide pressure. PaCO₂: arterial PCO₂. PtcCO₂: transcutaneous PCO₂. P_{ET}CO₂: end-tidal PCO₂.* Bias was the difference between PaCO₂ and PtcCO₂ or P_{ET}CO₂.

Table 4. Body temperature, hemodynamic parameters, arterial pH and haemoglobin level in PaCO₂ - PtcCO₂ non outliers *vs* outliers.

	Non outliers	Outliers	p
	n=51*	n=34*	
Body temperature, °C	37.7±0.6	37.9±0.9	0,63
Hemodynamic parameters:			
Capillary refilling time†, sec	2 (1-3)	2 (1-3)	0,35
Mottling, n(%)	23 (45%)	16 (47%)	1.0
Norepinephrine, µg/kg.min ⁻¹	0.46 ± 0.65	0.24 ± 0.3	0,39
Arterial pH	7.41±0.06	7.40 ± 0.05	0,48
Hemoglobin, g/dl	9.7±1.4	9.3±1.4	0,20

Values are expressed as mean±SD.*Number of pair data. † Data are expressed as median [interquartiles range].

Table 5. Body temperature, ventilation and hemodynamic parameters, and arterial PH in PaCO₂-P_{ET}CO₂ non outliers *vs* outliers.

	Non outliers	Outliers	p
	n=51*	n=34*	
Body temperature, °C	37.9±0.9	37.7±0.6	0,48
Ventilation parameters:			
- Respiratory rate, per min	13±2	14±4	0.53
- Tidal volume, ml/kg	7.9±1.3	7.6±1.0	0,48
- PEEP†, cm H ₂ O	3±2	4±2	0,33
Hemodynamic parameters:			
- Capillary refilling time††, sec	2 [1-3]	2 [1-3]	0.31
- Mottling, n(%)	21 (41%)	18 (53%)	0.40
- Norepinephrine, μg/kg.min ⁻¹	0.39±0.58	0.35±0.51	0,96
Arterial pH	7.41±0.06	7.4±0.05	0,41

Values are expressed as mean±SD unless otherwhise.*Number of pair data. †Positive end expiratory pressure. †† Data are expressed as median [interquartiles range].

Figure 1

