Ventilation Efficacy of Video-Laryngoscope Equipped With a Ventilation Feature

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INTRODUCTION: Achieving effective ventilation is challenging for anesthesia care providers and emergency medical personnel, as difficult mask ventilation and difficult intubation frequently occur. The aim of this study was to determine whether video-laryngoscopes equipped with a ventilation feature can produce effective ventilation. METHODS: An intubation mannequin with its trachea connected to a model lung with compliance 50 (normal compliance: C50) and 20 mL/cm H₂O (low compliance: C20) was used. Ventilation was established via a ventilation catheter (inner diameter 3.5 mm, 50 cm length) extending to the tip of the video-laryngoscope blade. Three different views of the vocal cords (grade 1, vocal cords fully visualized; grade 2, partial vocal cord visualization; grade 3, only epiglottis visualized) were tested. Ventilation was provided by jet ventilator (Jet). The Jet was operated at 10, 15, and 20 psi (Jet10, Jet15, and Jet20). Effective tidal volume (V_T) was defined as a V_T greater than anatomical dead space (150 mL). RESULTS: In C50, Jet15 and Jet20 generated effective V_T in all vocal cord views (for Jet15: grade 1, 663 \pm 33 mL; grade 2, 363 ± 25 mL; and grade 3, 198 ± 9 mL; for Jet20: grade 1, $1,005 \pm 114$ mL; grade 2, 484 \pm 38 mL; grade 3, 268 \pm 8 mL, respectively). In C20, Jet15 and Jet20 generated effective V_T in grades 1 and 2 (Jet15: grade 1, 288 ± 8 mL; grade 2, 160 ± 20 mL; grade 3, 81 ± 7 mL; Jet20: grade 1, 421 ± 20 mL; grade 2, 222 ± 16 mL; grade 3, 111 ± 8 mL, respectively). Jet10 achieved effective V_T in grade 1 and 2 (grade 1, 354 \pm 6 mL; grade 2, 223 \pm 37 mL, respectively) in C50 and grade 1 (163 \pm 12 mL) in C20. CONCLUSIONS: Video-laryngoscopes equipped with a ventilation feature provided effective V_T in simulated clinical scenarios. Further clinical study is required to validate these findings. Key words: video-laryngoscope; ventilation catheter; endotracheal intubation; difficult airway; emergency ventilation; jet ventilation. [Respir Care 2014;59(11):1-•. © 2014 Daedalus Enterprises]

Introduction

Difficult mask ventilation and intubation are major causes of morbidity and mortality in emergency and anesthesia care. Difficult tracheal intubation occurs in 1–4% of general surgical patients¹ and 4–11% in the emergency department.^{2,3} During field resuscitation, intubation is even more challenging.^{4,5} Intubation performed during chest compression and/or cervical stabilization in trauma pa-

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tients creates additional difficulty.^{6,7} The major cause of intubation-related brain damage or death is lack of adequate oxygenation and ventilation. The American Society of Anesthesiologists closed claim analysis of anesthesia complications indicates that respiratory-related events were responsible for 50% or more of the claims for death or

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permanent brain damage.⁸ In the respiratory events category, the most frequently seen events were difficult intubation (23%) and inadequate ventilation/oxygenation (22%).⁸ In addition, patients at risk for desaturation such as critically ill patients, obese patients, pregnant patients, and others show rapidly developing hypoxemia during intubation^{9,10} Therefore, it is important to minimize the apneic period, especially in patients at risk for desaturation, and to achieve effective ventilation during intubation, particularly when intubation is difficult or impossible. However, achieving these goals remains challenging for anesthesia care providers and emergency medical personnel.

Recently, video-laryngoscopes, enabling the operator to achieve better and quicker views than with direct laryngoscopes, have become available for use in operating rooms, intensive care units, and emergency departments.¹¹ Studies also demonstrated that video-laryngoscopes provide a higher intubation success rate than conventional laryngoscopes.11-13 However, it is unclear whether the use of video-laryngoscopes shortens the time to achieve successful intubation.^{14,15} Because the video-laryngoscope itself cannot provide adequate oxygenation and ventilation, better visualization of the vocal cords in the absence of quicker intubation may produce a false sense of security and does not translate into a reduction of hypoxia during intubation. In contrast, if ventilation is provided during intubation, it potentially avoids or minimizes hypoxia due to a lack of ventilation and affords the practitioner additional time to consider alternative airway management.

In this study, we evaluated a prototype of a videolaryngoscope equipped with the ventilation feature (VLs-Vent) using a jet ventilator (Jet). We hypothesized that the VLs-Vent would generate effective ventilation during endotracheal intubation. This hypothesis was tested on an intubation mannequin and lung model simulating respiratory system compliances potentially encountered in clinical scenarios.

Methods

Study Setup (Lung Model and Mannequin)

The study was conducted on an intubation mannequin (Laerdal Airway Management Trainer, Laerdal Medical, Stavanger, Norway) with its trachea connected to a lung model (Dual Adult TTL training/test lung, model 1600, Michigan Instruments, Grand Rapids, Michigan) (Fig. 1). The lung model had a functional residual capacity of 1,020 mL, and was connected to the distal end of an artificial trachea with anatomical dead space of approximately 150 mL. The lung model compliance was 50 mL/cm H₂O

OUICK LOOK

Current knowledge

During difficult tracheal intubation, oxygenation and ventilation can be compromised. A number of methods have been devised to maintain gas exchange during intubation.

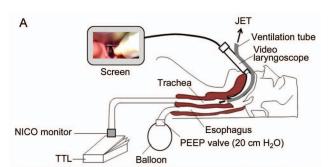
What this paper contributes to our knowledge

In a bench model, the use of high frequency jet ventilation with a modified video-laryngoscope allowed adequate tidal volume delivery with normal and low lung compliance with visualization of the vocal cords. When the vocal cords could not be seen and model lung compliance was low, ventilation was inadequate.

(normal compliance: C50) and 20 mL/cm H₂O (low compliance: C20). Airway resistance was set at 5 cm H₂O/L/s. A flow/pressure sensor (Nico cardiopulmonary management system, model 7300, Philips Respironics, Murrysville, Pennsylvania) was placed between the distal end of the mannequin trachea and the model lung (Fig. 1). The expiratory tidal volume (V_T), airway pressure, and gas flow were automatically recorded at a sampling rate of 100 Hz. To evaluate for gastric distention, the mannequin esophagus was connected to a PEEP valve, set at 20 cm H₂O, and a balloon (Fig. 1). The PEEP valve was unidirectional, only allowing air to enter the balloon. Before collecting data, the PEEP valve was tested ensuring that the balloon was inflated when positive-pressure ventilation was applied with a driving pressure greater than 20 cm H₂O.

Video-Laryngoscope Equipped With Ventilation Feature (VLs-Vent)

Ventilation was established by mounting a ventilation catheter extending to the tip of the blade of the video-laryngoscope positioned proximal to the vocal cords (Fig. 1). The ventilation catheter was a 19 Fr airway exchanger catheter (Cook Critical Care, Bloomington, Indiana) adjusted to 50 cm length (Fig. 1). Two different types of video-laryngoscopes, VividTrac (Vivid Medical, Palo Alto, California) and C-MAC (DL, Heine, Dover, New Hampshire), were tested. VividTrac has an angled blade, and an endotracheal tube was preloaded into the tube channel. The ventilation catheter was inserted into the endotracheal tube, and the distal tip of the ventilation catheter was advanced 1 cm ahead of the tip of the endotracheal tube (Fig. 1). C-MAC has a standard Macintosh blade (size 3)





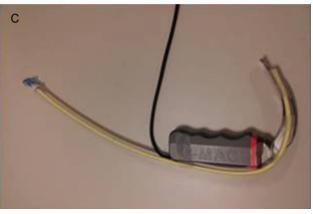


Fig. 1. Experimental setup and video-laryngoscope equipped with a ventilation feature. A: an intubation mannequin with its trachea connected to a model lung. The mannequin's esophagus was connected to a 20 cm $\rm H_2O$ PEEP valve and balloon. Ventilation catheter was connected to jet ventilator. NICO = noninvasive cardiac output monitor; TTL = lung model; JET = jet ventilator. B: ventilation catheter with VividTrac; C: ventilation catheter with C-MAC. The ventilation catheter was inserted into the endotracheal tube when VividTrac was used. The curvature of the endotracheal tube allowed the tip of the ventilation catheter to be aligned with the blade without any mounting. The ventilation catheter was taped to the C-MAC blade to direct the tip of the catheter in alignment with the blade.

and includes a camera. The ventilation catheter was attached to the video-laryngoscope parallel to the angle of its blade (Fig. 1). A jet ventilator (Jet, model 00-325, Anesthesia Associates, San Marcos, CA) was used to pro-

vide ventilation. The ventilation catheter was connected directly to the Jet. The Jet was operated at 10, 15, and 20 psi (68.9, 103.4, and 137.9 kPa) (Jet10, Jet15, and Jet20) at a breathing frequency of 15 breaths/min and inspiratory-expiratory (I:E) ratios of 1:3 and 1:1 achieved by the operator guided by a timer. Ventilation was performed with 3 different views of the vocal cords (grade 1, fully visible; grade 2, partially visible; and grade 3, not visible, with epiglottis only visualized) (Fig. 2).¹⁶

Data Collection and Analysis

Data from each experimental setting were continuously collected using the Nico Analysis Plus data management system. Establishment of a steady state was generally achieved after 2 or 3 breaths. Data were then collected, analyzed, and averaged from the next 10 consecutive breaths at each experimental setting. Data are presented as the mean \pm SD. Effective V_T was considered a V_T greater than anatomical dead space (150 mL). Continuous data from the lung simulator were compared using the Wilcoxon test to assess the impact of I-E ratio and lung mechanics on V_T. The Friedman test followed by Bonferroni correction for multiple comparisons was used for comparisons between driving pressure or different vocal cord views. Statistical analysis was performed with a statistical software package (PASW Statistic 18; SPSS, Chicago, Illinois). P < .05 was considered statistically significant. V_T differences are only reported if they are both statistically significant (P < .05) and clinically important (> 10%difference and differences of > 50 mL).

Results

Effects of Driving Pressure and View of Vocal Cords on $V_{\rm T}$ and Airway Pressure

As vocal cords were more visible and/or driving pressure increased, V_T increased (P < .001). V_T was larger in C50 than in C20 (P < .001). In C50, Jet15 and Jet20 generated effective V_T in all vocal cord views (Fig. 3). In C20, Jet15 and Jet20 generated effective V_T in grade 1 and grade 2 but not in grade 3 (Fig. 3). Jet10 achieved effective V_T in grade 1 and grade 2 in C50 and grade 1 in C20.

Figure 4 shows the peak airway pressure associated with each driving pressure and view of the vocal cords. As vocal cords were more visible and/or driving pressure increased, mean peak airway pressure increased (P < .001). Mean peak airway pressure did not differ significantly between C50 and C20. No gastric distention was observed with any driving pressure or view of the vocal cord.

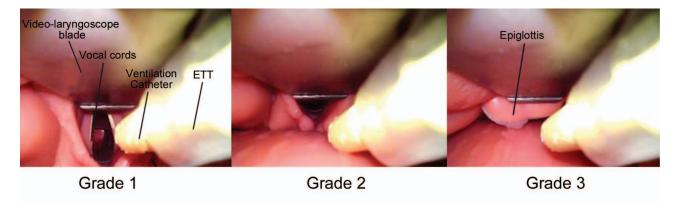


Fig. 2. Three views of the vocal cords taken with the VividTrac. Grade 1: vocal cords fully visible. Photo includes video-laryngoscope blade, vocal cords, endotracheal tube (ETT), and ventilation catheter. Grade 2: vocal cords partially visible; the center of screen was focused on the inlet of esophagus. Grade 3: vocal cords not visible; only the epiglottis is visualized.

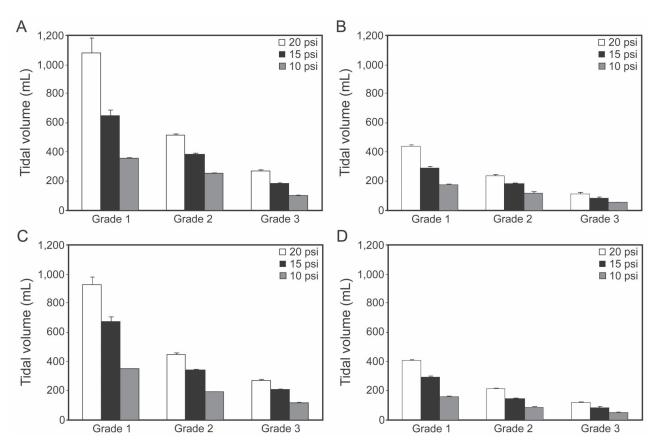


Fig. 3. Tidal volume at each driving pressure. A: VividTrac with normal compliance (50). B: VividTrac with low compliance (20). C: C-MAC with normal compliance (50). D: C-MAC with low compliance (20). Data are shown as mean \pm SD.

Effects of Ratios of Inspiration to Expiration Time on $V_{\rm T}$

There were no significant differences in V_T between I:E 1:3 and 1:1 in C50 (I:E 1:3 vs 1:1: grade 1, 639 mL

vs 710 mL; grade 2, 353 mL vs 360 mL; grade 3, 190 mL vs 194 mL; < 10% differences) and in C20 (I:E 1:3 vs 1:1: grade 1, 286 mL vs 296 mL; grade 2, 155 mL vs 164 mL; grade 3, 76 mL vs 86 mL; < 10% differences).

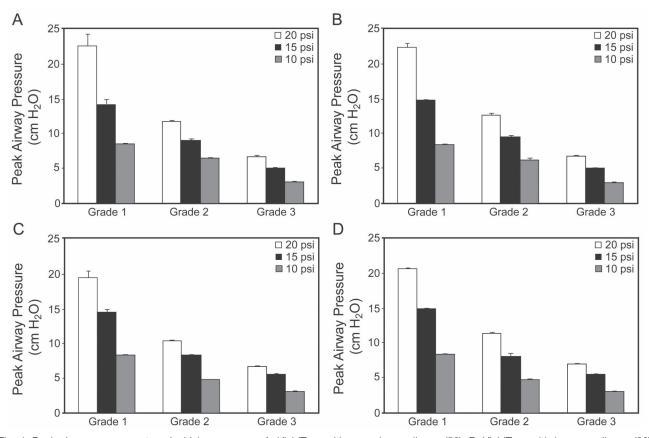


Fig. 4. Peak airway pressure at each driving pressure. A: VividTrac with normal compliance (50). B: VividTrac with low compliance (20). C: C-MAC with normal compliance (50). D: C-MAC with low compliance (20). Data are shown as mean ± SD.

Effect of Different Types of Video-Laryngoscope on $\boldsymbol{V}_{\boldsymbol{T}}$

There was no significant difference in V_T between the 2 types of video-laryngoscope in C50 (VividTrac vs C-MAC: grade 1, 698 mL vs 651 mL; grade 2, 389 mL vs 325 mL; grade 3, 190 mL vs 195 mL; < 10% differences) and in C20 (VividTrac vs C-MAC: grade 1, 300 mL vs 281 mL; grade 2, 177 mL vs 142 mL; grade 3, 81 mL vs 80 mL; < 10% differences or < 50 mL differences).

Discussion

The main findings of this study are as follows: (1) Jet15 and Jet20 can produce effective V_T with normal compliance in all views of vocal cords, (2) Jet15 and Jet20 can produce effective V_T with low compliance in grade 1 and grade 2 but not in grade 3, (3) Jet10 achieved effective V_T in grade 1 and grade 2 with normal compliance and grade 1 in low compliance, and (4) there were no differences in V_T between the 2 video-laryngoscopes. These preliminary data would indicate that a video-laryngoscope equipped with a ventilation feature can produce effective ventilation during intubation. To the best of our knowledge, this is the

first study to determine the efficacy of a prototype videolaryngoscope equipped with a ventilation feature.

In this study, the VLs-Vent achieved effective V_T even when the vocal cords were not visualized. One possible advantage of using the VLs-Vent is that upper airway patency is maintained by lifting the soft tissues directly and the location of the ventilation catheter can be clearly identified during intubation.

The effectiveness of ventilation generated by this device was strongly affected by the grade of vocal cord view and driving pressure. Compared with grade 1, V_T dramatically decreased in grade 2 and in grade 3. This may have been partially due to the mouth and upper airway being widely open, offering little resistance to gas leakage from the mouth. Our results are consistent with previous studies showing that, during supraglottic jet ventilation, incorrectly positioning the tip of the jet nozzle dramatically decreases effectiveness of ventilation compared with the nozzle positioned above the vocal cord opening. 17,18 Jet20 generated effective V_T in both normal and low compliance, but caused overinflation in normal compliance with grade 1 view ($V_T > 1,000 \, \text{mL}$). In contrast, Jet10 generated effective V_T in normal compliance model as long as the vocal

cords were partially or fully visible. In previous reports, supraglottic Jet ventilation with an endotracheal tube, combined with a 2.0 mm inner diameter ventilation tube and using 15 psi driving pressure, maintained adequate oxygenation and ventilation during tracheal intubation. 17,18 To generate an appropriate $\rm V_T$, driving pressure must be adjusted based on ventilation catheter location and patient's lung compliance. Considering that a grade 1 and grade 2 view can be obtained in 89–100% of cases with video-laryngoscopes, 14,19,20 we expect that our system may be useful and effective for ventilation during most intubations.

Percutaneous transtracheal jet ventilation (PTJV) has been recommended by the American Association of Anesthesiologists and Difficult Airway Society for management of the difficult airway during cannot intubate/cannot ventilate situations.^{21,22} However, a major concern with the use of jet ventilation via percutaneous transtracheal catheter is barotrauma or tissue damage. It has been reported that the incidence of barotrauma during PTJV is as high as 10%.23 These complications were mainly associated with incorrect insertion of the ventilation catheter. With our system, the operator can visualize the tip of the ventilation catheter during ventilation. Therefore, this system in combination with jet ventilation can provide ventilation as effective as PTJV, but it also prevents the damage caused by incorrect placement of the tip of the catheter. Another cause of injury during PTJV is that placement of the tip of the catheter is correct, but ventilation is provided when upper airway obstruction is complete.¹⁹ In such a case, intra-alveolar pressure can be as high as the driving pressure of jet ventilation. Therefore, catastrophic events may occur including pneumothorax^{23,24} and cardiac arrest²⁵ due to unrecognized upper airway obstruction during PTJV. In this new system, ventilation is performed via a video-laryngoscopy inserted into the pharyngeal cavity ensuring an open pathway. Therefore, the likelihood of barotrauma caused by unrecognized complete upper away obstruction is eliminated. In previous reports during supraglottic jet ventilation, driving pressure of 14.5-50.8 psi did not show any significant damage to pharyngeal tissue such as barotrauma or subcutaneous emphysema. 18,26

Another concern with this system is the development of gastric insufflation. In order to determine whether any significant gastric insufflation occurs when ventilation is provided with this system, we simulated lower esophageal sphincter opening pressure by placing a 20 cm H₂O PEEP valve on the esophagus (Fig. 1). Although airway pressure reached 22 cm H₂O with 20 psi driving pressure, significant gastric distention was not observed during ventilation. Because the opening pressure of the lower esophageal sphincter has been estimated to be approximately 20–25 cm H₂O under general anesthesia, ^{27,28} peak airway pressure

below 25 cm H₂O is unlikely to cause significant gastric insufflation. In previous reports, significant gastric insufflation was not observed during supraglottic ventilation, which is consistent with our results.^{17,18} However, there are some clinical situations where our device might induce gastric insufflations with high driving pressure, in any patient with an incompetent lower esophageal sphincter, such as after a cardiac arrest.^{29,30} Further clinical studies are needed to verify the safety of our device in these settings.

There are several limitations to this study. First, this study was not conducted in a real human, although the lung model and the intubation mannequin were adjusted to simulate adult clinical situations. Results from this study should be cautiously extrapolated to actual patient care until clinical studies can be conducted. Second, we only simulated an adult patient, and our study results may not apply to pediatric patients whose airway size and respiratory mechanics are quite different. Third, only 2 videolaryngoscopes were tested. Because the design features of individual scopes differ, all scopes should be evaluated before assuming results would be the same as ours. We believed that the efficacy of ventilation mainly depends on the distance from the tip of the ventilation tube to the vocal cords and the angulations of the nozzle as related to the tracheal axis.

In conclusion, the VLs-Vent can produce effective ventilation in the presence of normal respiratory system mechanics as long as the vocal cords are visualized. Because video-laryngoscopes provide a better view of vocal cords than direct laryngoscopes, this novel system can potentially improve ventilation/oxygenation during endotracheal intubation. Further clinical studies are needed to validate our observation, and to define specific design features and optimize its functionality.

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