

## Novel Oxygen-Concentrator-Based Equipment: Take a Test Drive First!

Patient incidents can teach us shocking and amusing lessons. The lesson may be obvious, but sometimes there is a second, subtler lesson. A recent incident involving new concentrator-based O<sub>2</sub> equipment provided both.

About 6 months ago, the afternoon therapist paged one of us to see a patient who was upset because the therapist would not fill his portable O<sub>2</sub> cylinder. His request and response were odd, because the practice of transferring *liquid* O<sub>2</sub> from large to small (portable) reservoirs at home is common, but that of transfilling *gaseous* O<sub>2</sub> from large to small cylinders has virtually disappeared.<sup>1</sup> While some local retailers fill their own small cylinders, none offers “while-you-wait” service. We, like everyone else, exchange full for empty cylinders. Our patient refused because his cylinder was special—a tiny size “A” and made of lightweight aluminum, it had an integrated *demand* valve and proprietary filling port that was incompatible with the threaded (CGA-540) and post-type (CGA-870) connectors on our large and small cylinders (Fig. 1).<sup>2</sup> Unsatisfied, he demanded to see a concentrator. When we showed how the tiny Diameter Index Safety System outlet also did not fit, he said he understood—we did not have the special pump. He grudgingly accepted the loan of an old-fashioned continuous-flow regulator and several full cylinders. We chatted as the therapist assembled the equipment for his drive home. He had spent most of the day at the center, visiting specialists. Suddenly, we realized that he had left home with a 3-hour O<sub>2</sub> supply for a 19-hour outing! He knew from his limited experience that the cylinder would last 3 hours, he had no spare (backordered from the manufacturer), and he extended his supply by shutting *off* flow while driving and sitting and used 1 L/min while walking, not the prescribed 2 L/min at rest and 3 L/min walking.

We will never forget our patient who was so enamored by the novelty of his home-filled O<sub>2</sub> cylinder that he *purposely* under-treated his hypoxemia. We smiled, reviewed the importance of complying with his prescription, discussed options for arranging adequate supplies, and sent him home with conventional equipment. Later, a report<sup>3</sup> about concentrator-produced O<sub>2</sub> raised concerns that we had missed a second, subtler lesson, namely, that clinicians and patients may *inadvertently* under-treat



Fig. 1. Invacare HomeFill II high-pressure cylinder with integrated demand valve and proprietary connector. The outlet nipple is not visible. The cylinder is placed horizontally before connecting to the high-pressure compressor. See Reference 2 for more details.

hypoxemia with this new equipment. We would like to discuss this potential problem: first, by describing novel concentrator-based equipment; next, by reviewing limitations of concentrators and associated demand valves; and last, by providing calculations to demonstrate these potential limitations.

**Novel Concentrator-Based Equipment. O<sub>2</sub> Cylinders Filled From Concentrators.** For decades, home concentrators have provided O<sub>2</sub> at low pressure. Recently, some vendors have used O<sub>2</sub> concentrators instead of cryogenic generators with *high-pressure compressors* to fill high-pressure cylinders. Now patients may use concentrators with high-pressure compressors to fill their cylinders at home.<sup>2,4,5</sup> One high-pressure compressor is an option for a proprietary concentrator, and a second is integrated with its proprietary concentrator. Both use cylinders with pro-



Fig. 2. Chad Total O<sub>2</sub>/Oxylite high-pressure cylinder, showing back of integrated pressure gauge, proprietary inlet hole (above cylinder neck to the right; plastic cover moved aside for illustration). Note that the CGA-870 post has 2 standard holes (Pin Index Safety System positions 2 and 5) for O<sub>2</sub> and a proprietary pin for use with proprietary demand valves. The cylinder is placed horizontally before connecting to the high-pressure compressor. See Reference 4 for more details.

proprietary connectors (see Figs. 1 and 2). The time to fill an empty cylinder varies considerably (eg, from about 75 min for a small “A” cylinder to more than 20 hours for an “E” cylinder) and depends on concentrator output, compressor capacity, and cylinder size. Cylinders can be used with a demand valve or conventional continuous-flow regulator.<sup>5</sup>

**Portable O<sub>2</sub> Concentrators.** Nearly 2 decades ago, a prototype briefcase-size, battery-powered O<sub>2</sub> concentrator that weighed less than 10 pounds amazed practitioners.<sup>6</sup> It provided 30% O<sub>2</sub>, so it would be considered an “enricher” today.<sup>1</sup> Recent technical advances have led to the production of 2 truly portable concentrators (ie, ≤10 pounds). Both can use an internal rechargeable battery, automobile 12-volt direct-current adaptor, or household alternating current, and they deliver *pulses of O<sub>2</sub>* with settings equivalent to continuous L/min flow.<sup>7</sup>

### Two Known Limitations of O<sub>2</sub> Delivery Equipment.

First, concentrators do not provide 100% O<sub>2</sub>. Under the best conditions, concentrators provide 96% O<sub>2</sub>.<sup>8</sup> Depending on design, state of repair, and *how close flow is set to the maximum rated flow*, the O<sub>2</sub> concentration can drop

substantially.<sup>8</sup> Some concentrators have sensors and alarms to indicate when concentration drops to a specific value, often in the range of 85–90%. Clinicians have ignored the consequences of less-than-pure O<sub>2</sub>, because of the shape of the hemoglobin-O<sub>2</sub> dissociation curve, limitations of pulse oximetry, and the ease of raising flow to compensate. In a recent report, half of the hypoxemic patients with chronic obstructive pulmonary disease (COPD) needed at least 1 (some 2 or 3) L/min *additional* O<sub>2</sub> flow from a concentrator to achieve the same P<sub>aO<sub>2</sub></sub> they had with cryogenically produced, 100%, “wall” O<sub>2</sub>.<sup>3</sup> This observation is relevant because many patients are assessed with 100% O<sub>2</sub> in a medical center but are sent home to use concentrator-provided O<sub>2</sub>.<sup>3</sup>

Second, equivalent-flow settings on O<sub>2</sub>-conserving pulse-dose demand valves are a fallacy.<sup>9</sup> Manufacturers take different approaches to determine the volume of the O<sub>2</sub> pulse (bolus) and *how the valve responds to changes in respiratory rate*. At the same “continuous O<sub>2</sub> equivalent-flow setting,” 3 different demand valves may deliver different O<sub>2</sub> volumes at a commonly observed respiratory rate (often 15 or 20 breaths/min), and as the respiratory rate increases, one valve *reduces*, a second *maintains*, and a third *increases* O<sub>2</sub> bolus volume. Experienced clinicians recognize that many hypoxemic patients must raise O<sub>2</sub> flow during exercise<sup>10</sup> to overcome the effects of increased demand and dilution with room air (air entrainment). In a recent bench evaluation, nearly all demand valves set at maximum flow demonstrated air entrainment with higher respiratory rate (ie, the delivered O<sub>2</sub> concentration dropped).<sup>11</sup>

In summary, compact and miniature O<sub>2</sub> concentrators will have less capacity than large traditional stationary concentrators and may provide less-than-pure O<sub>2</sub>. Depending on design, adding a conserving demand valve can mitigate or aggravate reduced O<sub>2</sub>-generating capacity. An unfortunate combination of low O<sub>2</sub> concentration and low O<sub>2</sub> bolus volume may lead to inadvertent under-treatment of hypoxemia, especially during exercise. Finally, it may not be possible to raise true (as opposed to equivalent) flow. That is, raising the equivalent flow may fail to achieve the desired effect. This potential limitation may be intuitively obvious to experienced clinicians. It will take time for bench and clinical studies to support or refute these concerns.

Until such studies are reported, one approach is to calculate the expected effects of air dilution on supplemental O<sub>2</sub> therapy with the *gas mixing equation*<sup>12</sup> (and personal communication, Alexander B Adams MPH RRT FAARC, Regions Hospital, St Paul Minnesota, and Peter L Bliss BME, Techniflow, Prior Lake, Minnesota; and OxyTec Medical, Anaheim Hills, California).

Table 1. Calculated Oxygen Concentrations Delivered by a Demand Valve With Pure Oxygen at Rest, Less-Than-Pure Oxygen at Rest, and Less-Than-Pure Oxygen With Reduced Volume During Exercise

L/min flow*	A			B			C		
	20 breaths/min at rest			20 breaths/min at rest			30 breaths/min during exercise		
	V <sub>ox</sub> (mL)	C <sub>ox</sub> (%)	C <sub>f</sub> (%)	V <sub>ox</sub> (mL)	C <sub>ox</sub> (%)	C <sub>f</sub> (%)	V <sub>ox</sub> (mL)	C <sub>ox</sub> (%)	C <sub>f</sub> (%)
"1"	10	100	22.6	10	95	22.5	06	95	21.9
"2"	20	100	24.2	20	90	23.8	12	90	22.7
"3"	30	100	25.7	30	85	24.8	18	85	23.3
"4"	40	100	27.3	40	85	26.1	24	85	24.1
"5"	50	100	28.9	50	80	26.9	32	80	24.8

The effect of dilution by air on calculated oxygen concentration (C<sub>f</sub>) is shown using an efficient demand valve (5:1 savings) with 100% O<sub>2</sub> (column A) and less-than-pure O<sub>2</sub> (column B) at rest, and, as designed, smaller volumes of less-than-pure O<sub>2</sub> (column C) during exercise. Note that C<sub>f</sub> is remarkably low when using an efficient demand valve (5:1 savings). One may draw a line to connect 3 similar C<sub>f</sub> values (italicized): 24.2% at equivalent flow "2" in column A, 24.8 at "3" in column B, and 24.8 at "5" in column C. The values for C<sub>f</sub> imply that using less-than-pure O<sub>2</sub> (eg, from a concentrator) requires at least one higher setting at rest than using pure O<sub>2</sub>. Of concern is that C<sub>f</sub> fails to rise during exercise, despite raising the "equivalent flow" by 3 settings, to the maximum "5". This is unfortunate because many patients have to raise true O<sub>2</sub> flow during exercise. This failure to provide higher O<sub>2</sub> concentration may under-treat hypoxemia.

\*L/min = equivalent flow setting

V<sub>ox</sub> = volume of oxygen delivered per breath

C<sub>ox</sub> = percent concentration of oxygen delivered per breath

C<sub>f</sub> = final concentration of oxygen delivered after considering dilution with air

Tidal volume = 500 mL = V<sub>ox</sub> plus inhaled air. See text for formula.

$$C_f = \frac{V_{ox} \times C_{ox} + V_{air} \times 21}{V_f}$$

where C<sub>f</sub> is the final O<sub>2</sub> concentration after accounting for air dilution, V<sub>ox</sub> is the volume (in mL) of delivered supplemental O<sub>2</sub>, C<sub>ox</sub> is the O<sub>2</sub> concentration (as a percent [eg, 100 for pure O<sub>2</sub>]), V<sub>air</sub> is the volume (in mL) of air entrained, 21 is the O<sub>2</sub> concentration (as a percent) of air, and V<sub>f</sub> is the sum of the volumes of supplemental O<sub>2</sub> and entrained air (ie, V<sub>f</sub> = V<sub>ox</sub> + V<sub>air</sub> = tidal volume).

For simplicity, we will fix tidal volume at 500 mL, so V<sub>air</sub> = 500 mL – V<sub>ox</sub>. If we plan to use a *hypothetical* demand valve that provides a 10-mL O<sub>2</sub> bolus at "1 L/min," 20 mL at "2 L/min," et cetera, up to 50 mL at "5 L/min," as determined by the manufacturer at 20 breaths/min (a commonly observed resting respiratory rate in patients with COPD), we may quickly calculate the final concentrations at each setting when using pure O<sub>2</sub> (C<sub>ox</sub> = 100). The results are summarized in Table 1 (column A).

The calculated final O<sub>2</sub> concentrations (C<sub>f</sub>) are remarkably low, ranging from 23% at setting 1 to 29% at setting 5. This is characteristic of an efficient O<sub>2</sub>-conserving demand valve that offers a 5:1 savings (eg, at setting 1, the valve provides 10 mL/breath × 20 breaths/min or 200 mL/min, a *fifth* of 1 L/min (1,000 mL/min) continuously flowing O<sub>2</sub>).

Next we can calculate the effect of using this efficient conserving demand valve with a *hypothetical* concentrator of limited capacity (ie, the O<sub>2</sub> concentration drops as flow setting rises). This might be either a portable concentrator or a high-pressure cylinder filled from a compact concentrator. Comparing C<sub>f</sub> with less-than-pure O<sub>2</sub> (column B in

Table 1) and with pure O<sub>2</sub> (column A in Table 1) suggests that flow will have to be raised by 1 setting; also, C<sub>f</sub> at setting 5 (maximum) using less-than-pure O<sub>2</sub> barely matches C<sub>f</sub> at setting 4 using pure O<sub>2</sub> (27%).

Last, we can calculate the effect of using less-than-pure O<sub>2</sub> with a demand valve that is designed to *reduce O<sub>2</sub> bolus volume* as respiratory rate rises (eg, at 30 breaths/min, a commonly observed respiratory rate during exercise in patients with COPD). The bolus is only 60% of that provided at 20 breaths/min (column C). Maximum C<sub>f</sub>, which is barely 25% at setting 5 (column C) matches C<sub>f</sub> at rest with setting 3 using less-than-pure O<sub>2</sub> (column B) and setting 2 using pure O<sub>2</sub> (column A). This *double reduction* of supplemental O<sub>2</sub> concentration and volume is *contrary* to the clinical experience that many patients with lung disease require higher O<sub>2</sub> flow during exercise to maintain arterial oxygen saturation.<sup>10</sup> This unfortunate combination may under-treat patients during exercise, despite raising equivalent flow to the maximum setting.

A more practical approach is to verify that the selected novel equipment provides adequate oxygenation during rest and exercise.<sup>10</sup> Manufacturers can design safety controls with sensors, alarms, and feedback circuits to provide minimum O<sub>2</sub> concentrations, but it is difficult to predict from published specifications if those less-than-pure O<sub>2</sub> concentrations, coupled with a demand valve, will actually provide what individual patients need.

Some buyers examine published fuel-economy ratings from the Environmental Protection Agency, while others scrutinize manufacturer's published performance specifications, but nearly all will take the chosen automobile for a test drive to see if it meets expectations. We think pa-

tients also deserve a “test drive” with the chosen novel compact and convenient O<sub>2</sub> equipment!

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#### REFERENCES

1. Kacmarek RM. Delivery systems for long-term oxygen therapy. *Respir Care* 2000;45(1):84–92.
2. Wilson PM. Making oxygen at home: the homefill concentrator. In: *Portable oxygen: a user's perspective*. <http://www.portableoxygen.org/march.html>. Accessed October 20, 2005.
3. Dheda K, Lim K, Ollivier B, Leftley J, Lampe FC, Salisbury A, et al. Assessments for oxygen therapy in COPD: are we undercorrecting arterial oxygen tensions? *Eur Respir J* 2004;24(6):954–957.
4. Wilson PM. Making oxygen at home: the total O<sub>2</sub> concentrator. In: *Portable oxygen: a user's perspective*. <http://www.portableoxygen.org/april.html>. Accessed October 20, 2005.
5. Cuvelier A, Nuir JF, Chakroun N, Aboab J, Onea G, Benhamou D. Refillable oxygen cylinders may be an alternative for ambulatory oxygen therapy in COPD. *Chest* 2002;122(2):451–456.
6. Akutsu T, Ishihara J, Wakai Y, Watanabe T, Yamaguchi M, Takubo T, et al. Development and clinical application of a portable oxygen concentrator. *Front Med Biol Eng* 1990;2(4):293–301.
7. Wilson PM. Concentrators: portable and transportable. In: *Portable oxygen: a user's perspective*. <http://www.portableoxygen.org/july.html>. Accessed October 20, 2005.
8. Johns DP, Rochford PD, Streeton JA. Evaluation of six oxygen concentrators. *Thorax* 1985;40(11):806–810.
9. McCoy R. Oxygen-conserving techniques and devices. *Respir Care* 2000;45(1):95–103.
10. Well D, Make B. Oxygen-conserving devices. In: O'Donohue WJ Jr, editor. *Long-term oxygen therapy, scientific basis and clinical application*. New York: Marcel Dekker; 1995:235–256.
11. Bliss PL, McCoy RW, Adams AB. Characteristics of demand oxygen delivery systems: maximum output and setting recommendations. *Respir Care* 2004;49(2):160–165.
12. Heurer AJ, Scanlan CL. Medical gas therapy. In: Wilkins RL, Stoller JK, editors. *Egan's fundamentals of respiratory care*. St Louis: Mosby; 2003:814.

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