The Site of Oxygen Delivery Into a Home Ventilator Affects Recorded Volumes

Erwan d'Aranda, Pierre-Julien Cungi, Quentin Mathais, Mickaël Cardinal, Pierre Esnault, Cédric Nguyen, Julien Bordes, Eric Meaudre, and Philippe Goutorbe

BACKGROUND: Long-term home mechanical ventilation is increasingly used by patients with chronic respiratory failure. Storage of medical data in the cloud is expanding, and ventilation can be monitored remotely. The aim of this bench study was to determine whether tidal volume (V_T) can be affected by the location of supplemental oxygen placement. METHODS: We tested 4 home ventilators in a bench test using a dual-chamber test lung to test the addition of supplemental oxygen placement via a connector in the circuit (ie, front intake port) versus via the manufacturer's rear intake port, with different oxygen supply flows of 2, 4, 6, and 8 L/min. We compared the effectively delivered V_T as measured with a pneumotachograph (ie, measured V_T) versus the V_T reported by each home ventilator (ie, monitored V_T). RESULTS: For all of the home ventilators, the monitored V_T and measured V_T were comparable when the rear oxygen intake was used, regardless of oxygen flow. However, when the front oxygen intake was used, the monitored V_{T} as measured by the ventilators was significantly lower than the measured ${
m V_T},$ with the greatest difference reaching 29% for the highest oxygen flow tested (8 L/min). CONCLUSIONS: The monitored V_T may be inaccurate if oxygen is added with a connector in the circuit, which may have consequences on both the individual level and collective level (ie, big data analysis). Physicians who analyze data from home ventilators should be aware of the site of oxygen supplementation and promote use of only the rear oxygen intake. Key words: home ventilator; oxygen administration; tidal volume; telemonitoring; cloud; bench test. [Respir Care 2020;65(3):288–292. © 2020 Daedalus Enterprises]

Introduction

Long-term home mechanical ventilation is increasingly used by patients with chronic respiratory failure.

In a recent study, Masefield et al² summarized the prev-

Drs d'Aranda, Cungi, Mathais, Cardinal, Esnault, Meaudre, and Goutorbe are affiliated with the Intensive Care Unit, and Drs Nguyen and Bordes are affiliated with the Anesthesia Department, Sainte Anne Military Teaching Hospital, Toulon, France. Dr Meaudre is also affiliated with the French Military Health Service Academy Unit, Ecole du Valde-Grâce, Paris, France.

The authors have disclosed no conflicts of interest.

Correspondence: Erwan d'Aranda MD, Hôpital d'Instruction des Armées Sainte Anne, Service de Réanimation, BP 600, 83800 Toulon Cedex 9, France. E-mail: erwan.daranda@gmail.com.

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alence from several surveys: 12.9 per 100,000 in a Canadian report,³ and 9.9 and 12 per 100,000 in Australia and New Zealand, respectively.⁴ The latter study of 2,725 subjects showed that a pressure targeted mode was used in 95.5% of cases. Home ventilators are pressure ventilators and, in most cases,⁵ use a turbine. The turbine generates flow, which is regulated to maintain the required pressure via feedback from pressure sensor. The volume generated should be monitored because it varies with the patient's breathing patterns (ie, compliance, resistance, and muscle effort).

Patients often benefit from supplemental oxygen to improve gas exchange. Oxygen is often delivered through an orifice on the ventilator or by a T-piece positioned in the patient circuit. The single-limb circuit may be preferred over the dual-limb circuit because it is less cumbersome for the patients, even if the expiratory volume cannot be monitored. A number of home ventilators on the market do not have a rear oxygen port. To our

knowledge, no one has studied the influence of the site of oxygen supplementation on the monitored tidal volume (V_T). Therefore, we analyzed the volume actually delivered to the patient and the volume indicated by the home ventilator by varying the location of oxygen intake and oxygen flow on a test lung.

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Methods

This experimental study was carried out as a bench test as described by Aslanian et al,6 consisting of a dual test lung (adult/infant lung simulator, Michigan Instruments, Grand Rapids, Michigan) (Fig. 1). Each tested ventilator was connected by a single-limb circuit with a ventilatorcontrolled exhalation valve (without leaks during inspiration) to the first chamber of the test lung. The 2 chambers were physically connected by a small metal component that allowed the driving chamber to lift the testing chamber. The second chamber (ie, the driving chamber) was pressurized by a ventilator (PB 840, Puritan Bennett, Covidien), which was recognized as an inspiratory effort by the tested ventilator. The drive ventilator was set at a breathing frequency of 15 breaths/min and inspiratoryexpiratory ratio of 1:2. Oxygen supplementation was provided at either the back of the ventilator as recommended by the manufacturer (ie, the rear intake port), or via a T-piece positioned between the ventilator and the patient circuit (ie, the front intake port). The oxygen flow was regulated by a precision flow meter (FlowAnalyser PF-300; imtmedical, Buchs, Switzerland). Measured V_T was determined using a pneumotachograph between the patient circuit and test lung (Fleisch 6V, Lausanne, Switzerland), and was recalibrated between each ventilator tested. Lung resistance was 20 cm H₂O/L/s, and a compliance of 60 mL/cm H₂O was applied to the test lung.

We studied 4 models (different serial numbers) of 4 ventilators: Legendair (Covidien [AIROX], Dublin, Ireland), PB560 (Covidien, Mansfield, Massachusetts), Vivo50 (Breas Medical, Mölnlycke, Sweden), and Trilogy 100 (Philips, Eindhoven, The Netherlands). The ventilator settings were patient-initiated and -terminated breaths with a PEEP of 5 cm $\rm H_2O$ and inflating pressure of 10 above PEEP. We studied 4 oxygen supply flows: 2, 4, 6, and 8 L/min. For each oxygen flow, we noted the $\rm V_T$ delivered by the home ventilator (ie, monitored $\rm V_T$) and the $\rm V_T$ effectively received by the patient on the pneumotachograph (ie, measured $\rm V_T$). Oxygen bleed-in was carried out once at the back of the ventilator and once at the front. Each measurement was repeated 5 times (one sequence is one measure for each oxygen flow).

QUICK LOOK

Current knowledge

Use of cloud storage for medical data is expanding, and ventilation can be monitored remotely as home ventilator use increases. Supplemental oxygen placement can be delivered via a connector in the circuit or the ventilator's rear intake port. The site of oxygen supplementation can affect delivered tidal volume.

What this paper contributes to our knowledge

On a home ventilator, when oxygen was added with a connector in the circuit, the monitored tidal volume falsely decreased. Physicians who analyze data from home ventilators should be aware of the site of oxygen supplementation and avoid oxygen bleed-in via the inspiratory limb.

This study was performed at Sainte Anne Military Teaching Hospital, Toulon, France, and the ethics review board of this institution approved the research protocol.

Statistical Analysis

Quantitative data are given as mean (SD). V_T and oxygen flow for each oxygen admission were compared with 2-way covariance analysis (ANOVA test). Tests were repeated for each ventilator. P < .05 were considered significant. For each home ventilator model, we compared the measured V_T and the monitored V_T .

Results

For each ventilator, the mean difference between the volume indicated by the tested home ventilator and the volume received by the test lung (PB560, 5.7%; Vivo50, 2.7%; Legendair, 8%; Trilogy, 6.7%) were lower than the 10% standard (F1246-91 of the American Society for Testing and Materials; https://www.astm.org/Standards/F1246.htm, *Accessed August 29, 2019*).

For all ventilators, the monitored V_T and measured V_T were comparable when the rear oxygen intake was used, regardless of oxygen flow. In contrast, the monitored V_T was significantly lower than the measured V_T when the front oxygen intake was used. This difference begins with 2 L/min and increases to 29% with increased oxygen flow. Data for the tests with the Vivo50 are presented in Table 1 as an example. To combine all of the measurements, we expressed the results in variations of measured V_T and monitored V_T . The baseline

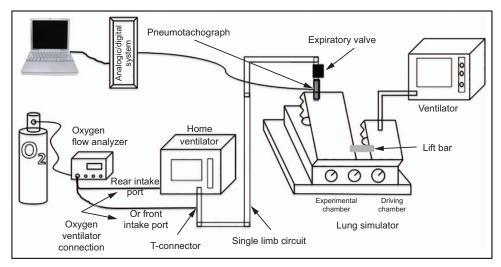


Fig. 1. Experimental setup.

 $\begin{array}{ll} \mbox{Table 1.} & \mbox{Measured } \mbox{V_T and Monitored V_T With the Vivo50} \\ & \mbox{Ventilator According to Oxygen Admission Location} \end{array}$

O ₂ Flow, L/min	Measured V_T , mL	$\begin{array}{c} \text{Monitored} \\ \text{V}_{\text{T}}, \text{ mL} \end{array}$	P
Rear intake port			.20
2	543.3 ± 39.9	556.9 ± 30.9	
4	551.7 ± 40.8	551.7 ± 32.7	
6	559.2 ± 39.7	549.1 ± 33.8	
8	566.0 ± 40.0	545.4 ± 35.3	
Front intake port			< .01
2	546.3 ± 40.7	522.1 ± 27.2	
4	554.7 ± 40.7	481.9 ± 25.0	
6	564.0 ± 39.8	436.6 ± 26.1	
8	571.0 ± 40.4	401.1 ± 21.1	

 V_T = tidal volume

(100%) was measured $V_{\rm T}$ with 2 L/min oxygen flow on the rear intake port (Fig. 2).

Discussion

This bench study shows that the site of supplemental oxygen intake influences the monitored V_T . When oxygen bleed-in is introduced after the ventilator flow sensor (ie, via the front intake port), the monitored V_T is minimized although the real V_T remains the same. In the case of a higher oxygen flow, this error could reach 29% (eg, with the Trilogy 100 and the Vivo50 at 8 L/min O_2). However, we found no difference between the monitored V_T and measured V_T when the rear intake was used. These findings may be explained by the intake's position after the ventilator flow sensor, meaning

this flow cannot be measured even though the oxygen flow is part of a patient's V_T .

During volume control, the addition of oxygen flow in the inspiratory limb increases the V_T , whereas with pressure control, the inspiratory pressure target is obtained earlier and the ventilator indicates a lower V_T than the actual V_T received by the patient. This study used a single-limb valve circuit, which is currently used for tracheostomized patients. This group represents $\sim 10\%$ of home mechanical ventilation in a European study.⁵ In this case, the difference between monitored and actual V_T could prove harmful.

With a single-limb leak circuit for noninvasive ventilation, the difference should be low (ie, the influence of oxygen is reduced by the leakage rate, which can reach 60 L/min). Further, oxygen flow would be reduced secondary to total leak. Ventilators that do not have a rear oxygen intake should not be used in tracheostomized patients, although they could still be used as rescue ventilators. Another bench study has reported that V_T may be underestimated to varying extents by home ventilators.

Internal memory data from a ventilator can be reviewed by a clinician to assess the efficacy and tolerance of the ventilation. ^{10,11} Moreover, the use of telemonitoring patients' home ventilator patterns is growing. ¹² If the physician cannot see the location of the oxygen input, misinterpretation of the monitored V_T could lead to incorrect pressure increases, leading to overinflation and generating intrinsic PEEP or unloading respiratory muscles. For example, at the individual level, a physician reading a remotely monitored mean V_T of 400 mL for a adult male patient ventilated in pressure-support mode could consider increasing the level of the pressure support, which would not be indicated if the actual mean

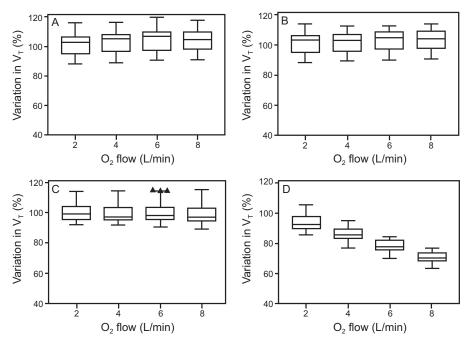


Fig. 2. Variations in measured (A and C) and monitored (B and D) tidal volume (V_T) according to oxygen admission location for all tested home ventilators. A: Measured V_T , rear intake port, B: monitored V_T , rear intake port, C: measured V_T , front intake port, and D: monitored V_T , front intake port. Triangles indicate height values.

 $V_{\rm T}$ is 520 mL, a difference that could occur in the worst-case scenario. If the patient experiences air trapping, increasing the pressure level is not the best solution.

At a collective level, results of big data studies would be incorrect. Manufacturers with the main share of the home ventilator market and cloud data management may be able to analyze rapidly a large cohort of tracheostomized receiving volume ventilation. For example, with a breathing frequency of 10 breaths/min, an inspiratory-expiratory ratio of 1:2, and 3 L/min O₂ for each V_T, 100 mL is added to the oxygen flow. Is a 100-mL error acceptable for monitoring V_T, especially to determine whether a home ventilator is effective? Exploiting these inexact data through big data may lead to the risk of inexact conclusions for carbon dioxide or a survival end point. The limitations of our study are related to the bench test and extrapolation to patients.

Conclusions

Physicians who analyze data from home ventilators should promote the use of only the rear oxygen intake. V_T and minute volume may be underestimated when oxygen is added with a connector in the circuit (ie, the front oxygen intake), which may have damaging consequences at both the individual level and collective level (ie, big data analysis).

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